



# Gastric floating in-situ gel as a strategy for improving anti-inflammatory activity of meloxicam

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## ABSTRACT

The present study was aimed to develop gastric floating in-situ gels of meloxicam (MLX) mainly to enhance anti-inflammatory activity and alleviate gastric ulceration potential of meloxicam. Ternary inclusion complex of meloxicam containing hydroxypropyl beta cyclodextrin (HP $\beta$ CD) and diethylamine (DEA) in 1:1:1 molar ratio was used as a chief component in the development of gastric floating *in-situ* gel formulations of meloxicam. Box–Behnken design was utilized to design and optimize gastric floating *in-situ* gels of meloxicam. Independent variables (concentrations of sodium alginate, calcium carbonate, and a ternary inclusion complex of meloxicam, respectively) were optimized in order to achieve the desired responses. The response surface plots and the possible interactions between the independent variables were analyzed using the Design Expert Software 11.0.3.0 (Stat-Ease, Inc, USA). The results showed that the optimized gastric floating in-situ gels with a short floating lag time (41 seconds), low viscosity (190 cps), and high *in vitro* drug release at sixth hour (77%) was obtained using an optimized combination of calcium carbonate (0.75% w/v), sodium alginate (1.25% w/v), and MLX-HP $\beta$ CD-DEA ternary complex (equivalent to 11.25 mg of meloxicam), respectively. Moreover, the optimized gastric floating in-situ gel formulation of meloxicam ternary complex exhibited significantly ameliorated anti-inflammatory activity [84.38% ( $p < 0.05$ ) at sixth hour and also showed a significant reduction in local gastric ulceration potential compared to pure meloxicam]. Thus, this gastric floating in situ gelling system can be translated for existing and established non-steroidal anti-inflammatory drugs (NSAID) as well as formulations.

## INTRODUCTION

Oral liquids offer several advantages over other oral pharmaceutical formulations such as tablets, capsules, and pills but they often suffer from abrupt gastrointestinal transit. This could be a serious concern for the majority of drugs, particularly weakly acidic drugs as they are absorbed from the stomach and/or upper part of the small intestine (El-Kamel *et al.*, 2001; Rouge *et al.*, 1996). The gastric retention of oral solutions containing these drugs could be favorably achieved through a radical approach of the liquid in-situ gelling system. These systems are polymeric gel formulations

that respond to physical or chemical signals, including pH, ionic factor, metabolite, or temperature (Kubo *et al.*, 2003; Miyazaki *et al.*, 2001; Prabakaran and Mano, 2006). Numerous polymers such as pectin (Ghare and Mundada, 2017), chitosan (Belhadji *et al.*, 2017), gellan gum (Kerdsakundee *et al.*, 2016), xyloglucan, and xanthan gum have been investigated for this purpose. Sodium alginate is a linear block polysaccharide copolymer made of  $\beta$ -D-mannuronic acid (M) and  $\alpha$ -L-guluronic acid (G) residues joined by 1,4 glycosidic linkages. It undergoes gel formation by virtue of temperature change or because of the presence of cations (e.g., Na<sup>+</sup>, K<sup>+</sup>, Ca<sup>2+</sup>). It is a water-soluble polysaccharide. It produces a gel via formation of double helices, followed by their ionic cross-linking. Incorporation of suitable amounts of gas-forming substance like calcium carbonate to the aqueous solutions of the above polymers could make them float on the surface of the gastric fluid (Rajinikanth *et al.*, 2007). This floating property of the gels could help in enhancing clinical response and also minimizing the

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gastric irritant effect of weakly acidic drugs by preventing direct contact with the stomach mucosa (Thanoo *et al.*, 1993).

Over the years, substantial work mainly related to the meloxicam-cyclodextrin and/or hydrophilic excipient complex/dispersion incorporated formulations such as tablets (Samprasit *et al.*, 2015), suspension (Awasthi *et al.*, 2011), suppositories (Gowthamarajan *et al.*, 2002), and buccal patches (Jafar and Ali, 2011) has been reported in the literature. However, except our past work (Jafar *et al.*, 2017), there is a lack of major evidences in the literature about the meloxicam ternary complex (prepared using cyclodextrins and alkali substance combination) incorporated gastric floating in-situ gels, even though this has been considered to be very beneficial from the therapeutic point of view.

Therefore, the present study was planned to develop meloxicam ternary complex incorporated gastric floating in-situ gels to improve *in vivo* anti-inflammatory activity and reduce local ulceration potential of meloxicam. Box–Behnken design (Box and Wilson, 1951), which gives small number of experimental runs and takes less time, and thus, offers a far more effective approach than the traditional approaches concerning statistical optimization of a pharmaceutical formulation (Alam *et al.*, 2016) was used in the design of gastric floating in-situ gels of meloxicam-hydroxypropyl beta cyclodextrin-diethanolamine ternary complex.

## MATERIALS AND METHODS

### Materials

Meloxicam is purchased from the UFC Biotechnology New York (USA), Sodium alginate and calcium carbonate were purchased from the Research Lab Fine Chemicals, Mumbai (India), while other ingredients used were of analytical research grade.

### Preparation of gastric floating in-situ gels

Gastric floating in-situ gels of meloxicam (MLX)-hydroxypropyl beta cyclodextrin (HPβCD)-diethylamine (DEA) ternary complex were prepared as per the reported method (Shendge *et al.*, 2014). Weighed quantity of sodium alginate was transferred to a beaker containing half of the total volume of double distilled water, which contains 0.25% w/v of sodium citrate. The contents of the beaker were heated to 90°C with continuous stirring on a magnetic stirrer until a clear solution was obtained and then the solution was allowed to cool below 40°C. Calculated amounts of calcium carbonate and MLX-HPβCD-DEA ternary complex were dissolved in the second half of the double distilled water in a separate beaker and this solution was slowly added with

continuous stirring to the cooled sodium alginate solution. Finally, the in-situ gelling solution obtained was stored in an amber colored glass bottle in a cool place until further investigation.

### Optimization

Based on our previous published work (Jafar *et al.*, 2018), MLX-HPβCD-DEA ternary complex (1:1:1 molar ratio) was selected as one of the factors influencing the performance of gastric floating in-situ gels of meloxicam. The other two independent variables or factors, i.e., calcium carbonate and sodium alginate were selected based on factor screening study. The Box–Behnken experimental design was employed to optimize the floating in-situ gelling solutions wherein the concentrations of calcium carbonate (A), sodium alginate (B), and MLX-HPβCD-DEA ternary complex (C) were selected as independent variables or factors. Each factor was kept as low, medium, and high levels. Floating lag time, viscosity, and percent cumulative drug release at sixth hour were taken as dependent variables or responses (Table 1). The effect of factors on the observed responses was analyzed employing Design expert version 11.0.3.0 (Stat-Ease, Inc, USA) software. Fifteen experimental runs obtained from the design with three middle points with their observed responses are depicted in Table 2. The responses were statistically analyzed by the analysis of variance (ANOVA) test method. The optimum formulation was chosen by the numerical optimization process using the desirability function. In order to assess the impact of each factor on the observed responses, the polynomial coefficients for in-situ gelling solutions were ascertained. The polynomial equation generated by this experimental design is as follows:

$$Y = b_0 + b_1A + b_2B + b_3C + b_{12}AB + b_{13}AC + b_{23}BC + b_{11}A^2 + b_{22}B^2 + b_{33}C^2$$

Where  $Y$  is the response;  $b_0$  is the intercept;  $b_1$ – $b_{33}$  are the regression coefficients calculated from the observed experimental values; and  $A$ ,  $B$ , and  $C$  are the coded levels of the factors. The terms  $A$ ,  $B$ , and  $C_i^2$  ( $i = 1, 2, \text{ or } 3$ ) constitute the interaction and quadratic terms, respectively.

### In-vitro evaluation of gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex

#### Appearance

The color and the clarity of the gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex were evaluated by the visual inspection of the solutions against a dark illuminating background.

**Table 1.** Variables in a Box–Behnken design for the formulation of gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

Factors	Level used, actual coded		
	Low (-1)	Medium (0)	High (+1)
<b>Independent variables</b>			
A = calcium carbonate (%)	0.25	0.5	0.75
B = sodium alginate (%)	1.25	1.75	2.25
C = MLX-HPβCD-DEA≡ meloxicam (mg)	7.5	11.25	15
<b>Dependent variables</b>		Goals	
$Y_1$ = floating lag time (Sec)		Shorten	
$Y_2$ = viscosity (cps)		Decrease	
$Y_3$ = cumulative drug release (%)		Enhance and prolong	

**Table 2.** Observed response in Box–Behnken design for gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex.

Run no.	Variables*			Responses		
	A	B	C	Floating lag time	Viscosity	Cumulative drug release
	%w/w	%w/w	mg	(Seconds)	(cps)	(%)
1	0.25	1.25	11.25	340	1,160	54
2	0.25	1.75	15	334	472	72
3	0.75	2.25	11.25	54	1190	52
4	0.25	1.75	7.5	342	430	69
5	0.5	2.25	15	174	1,180	55
6	0.5	1.75	11.25	170	440	61
7	0.75	1.25	11.25	41	190	77
8	0.25	2.25	11.25	338	1,150	59
9	0.75	1.75	7.5	51	413	71
10	0.5	1.75	11.25	170	440	61
11	0.5	2.25	7.5	160	1,130	57
12	0.5	1.25	15	160	210	77
13	0.5	1.25	7.5	180	170	75
14	0.5	1.75	11.25	170	440	61
15	0.75	1.75	15	50	420	66

\*A = calcium carbonate; \*B = sodium alginate; \*C = MLX-HP $\beta$ CD-DEA ternary complex.

#### *pH measurement*

The pH of gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex was measured by a calibrated digital pH meter (HI-2214 logging pH bench meter, UK) at room temperature using 30 ml of the sample. The pH determination for each sample was performed in triplicate.

#### *Viscosity measurement*

The viscosity of gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex was determined by a Viscometer (SV-10 Japan) at a room temperature using 30 ml of the sample. Viscosity determination for each sample was done in triplicate.

#### *In-vitro gelation study*

*In vitro* gelation study was conducted on gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex as described in the literature (Sharma *et al.*, 2014). Ten milliliter of the gelling solution was transferred to 500 ml of 0.1 N HCL (pH 1.2) in a beaker without much turbulence to prevent shattering of the formed gel. Gelling was observed in the beaker by visual inspection and the formulations based on their gelling consistency were given with different grades.

#### *In-vitro floating study*

*In vitro* floating study of in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex was conducted as per the method reported in the literature (Rajnikanth and Mishra, 2009). Five hundred milliliter of the dissolution medium (pH 1.2) is taken in a dissolution flask (USP Type-II) and the temperature of the dissolution medium was maintained at 37°C  $\pm$  0.5°C. Ten milliliter of the solution is transferred to a Petri dish (4.5 mm internal diameter) and the Petri dish is carefully placed at the bottom of a dissolution flask without much disturbance in the flask. The time taken by the in-situ gel to come up to the surface of the medium (floating lag time) and also about how much time the gel continuously floated on the surface of the medium (duration of floating) was recorded.

#### *In-vitro drug release study*

*In vitro* release of meloxicam from the gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex was determined in a USP XXIV rotating paddle apparatus (eight basket Dissolution Test Station, Electrolab, India) at 37°C using the paddle method at 50 rpm/minute. The dissolution medium used was 500 ml of 0.1 N Hydrochloric acid (pH 1.2) which was prepared and degassed using a media preparator (EMP-21 DO, Electrolab, India). The in-situ gel is added to a Petri dish (4.5 mm internal diameter) and the Petri dish is then transferred to the bottom of a dissolution basket without much disturbance. Five milliliter samples were withdrawn at fixed time intervals and analyzed at 362 nm using UV-Visible Spectrophotometer (BT-600 UK). After each withdrawal, an immediate replacement of 5 ml fresh dissolution medium was done to maintain a sink condition. Each determination was performed in triplicate till 6 hours.

#### *In-vivo activity*

The *in vivo* activity experimental protocol was approved by the Institutional Review Board and Animal Ethical Committee of the Imam Abdul Rahman Bin Faisal University (formerly University of Dammam), Dammam, Kingdom of Saudi Arabia (Approval number: IRB-2014-3-199).

#### *Animals*

Wistar rats of either sex weighing 200–250 g were used in the present study. The selected animals were housed in polypropylene cages under standard laboratory conditions (temperature 25°C + 2°C) with a cycle of 12 hours of darkness and light. The animals were fed with standard diet and water *ad libitum* and were fasted for at least 12 hours prior to the anti-inflammatory activity experiment.

#### *Carrageenan-induced rat hind paw edema method*

Carrageenan-induced rat hind paw edema method (Winter *et al.*, 1968) was used to assess the anti-inflammatory activity of

optimized gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex. Rats were divided into three groups; each group has six rats. The animals of group I received 1 ml of control [Calcium carbonate/sodium alginate (0.75% w/v/1.25% w/v)] per oral and groups II and III received per oral Standard [Calcium carbonate/sodium alginate/pure meloxicam (0.75% w/v/1.25% w/v/11.25 mg)] and optimized gastric floating in-situ gel [Calcium carbonate/sodium alginate/(0.75% w/v/0.25%w/v/MLX-HP $\beta$ CD-DEA ternary complex equivalent to 11.25 mg of meloxicam)], respectively (Dose of meloxicam: 1 mg/kg body weight). After 1 hour of the test drug administration and the control treatment animals of groups I, II, and III were injected with subcutaneous injection of 0.1 ml of 1% w/v solution of carrageenan (Sigma Chemical Co, St. Louis, MO) in normal saline into the plantar side of the left hind paw. Plethysmograph (UGO Basile, Italy) was used to measure the rat paw volume. The paw volume was measured at 0, 1,2,3,4, and 6 hours after the injection of carrageenan.

The edema inhibitory activity was computed using the following formula:

$$\% \text{ edema inhibition} = (1 - D/C) 100$$

Where,

*D*-represents the percentage difference in increased paw volume after the administration of test drugs to the rats.

*C*-represents the percentage difference of increased volume in the control groups.

#### Ulcerogenic study

For the gastric mucosal damage studies, rats were not fed for 24 hours but the water was made available to them. The rats of the control group were given normal saline, the standard drug group were given 15 mg/kg body weight of meloxicam standard drug, and the formulation group were given 15 mg/kg body weight of optimized gastric floating in-situ gel of meloxicam. All the rats were euthanized 4 hours after the drug administration and stomachs were excised and were cut open along the greater curvature from the oesophagus to the pylorus. Stomachs were placed on a corkboard and pinned, the ulcer score was done by examining under the dissection microscope. A blind observer unaware of the experimental groups was requested to assess the mucosal damage. Scoring sheet (Mishra and Vijay Kumar, 2006) containing the following rubrics was used for scoring

- 0—no injury or bleeding
- 1—slight injury (two to three dots)
- 2—severe injury (hemorrhagic streaks, five to six dots)
- 3—very severe injury (many lined injuries)
- 4—mucosa full of lesions

#### Statistical analysis

For ulcer scoring study, we used SPSS version 23. The data are expressed as mean  $\pm$  SE. One ANOVA was performed to compare between groups followed by Tukey's post hoc test. *p* value < 0.05 was considered significant.

## RESULTS AND DISCUSSION

### Optimization

Fifteen gastric floating in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex were developed according to the experimental

design and characterized by different responses such as floating lag time, viscosity, and drug release. The mathematical correlations were set up and coefficients of the second order polynomial equations were derived using multiple linear regression analysis for a floating lag time, viscosity, and drug release were found to be quadratic in nature with interaction terms. The coefficients of the polynomials fit well to the data, with the values of *R*<sup>2</sup> ranging between 0.4373 and 0.9957 (*p* < 0.005 in all cases). The three dependent values ranged from 41 to 342 seconds, 170–1,190 cps, and 52%–77% for a floating lag time, viscosity, and drug release, respectively. A positive value in polynomial equations corresponds to an effect that favors the optimization, whereas a negative value represents an inverse relationship between the factor and the response. The polynomial equations derived from the statistical analysis of the results are given in Table 3. Where *A*, *B*, and *C* correspond to the coded values of the calcium carbonate, sodium alginate, and meloxicam, respectively. The effect of calcium carbonate on floating lag time is comparatively more significant than the effect of sodium alginate. Other independent variable meloxicam has not shown any significant change in the floating lag time of in-situ gelling solutions. All three independent variables, namely calcium carbonate, sodium alginate, and meloxicam individually and also in combinations showed the positive effect on viscosity. But the effect of the said variables is negative on drug release. This could be due to the sol to gel transformation of the formulations in an acidic medium.

All the responses studied for 15 in-situ gel formulations were collectively fitted to various models using Design expert version 11.0.3.0 (Stat-Ease, Inc, USA). The best-fitted model of the three factors and their comparative values of *R*<sup>2</sup>, predicted *R*<sup>2</sup>, adjusted *R*<sup>2</sup>, standard deviation (SD), and %CV are given in Table 3. The “predicted *R*<sup>2</sup>” was more or less in accordance with the “adjusted *R*<sup>2</sup>” values (Fig. 1). The 3D response surface graphs presenting the interaction effects of the factors on the responses are illustrated in Figure 2. The fitting results showed that the optimized in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex with short floating lag time (41 seconds), low viscosity (190 cps), and high drug release at the sixth hour (77%) was obtained using an optimized combination of calcium carbonate (0.75% w/v), sodium alginate (1.25% w/v), and meloxicam content (11.25 mg), respectively. All the response surfaces were best fitted with quadratic polynomial models and are capable of predicting the interaction effects as well. Finally, the model was analyzed for ANOVA (*p* < 0.005), which disclosed that the model terms for main effects and interaction effects were highly significant.

### In-vitro evaluation of gastric floating in-situ gels

All 15 in-situ gels of MLX-HP $\beta$ CD-DEA ternary complex were clear, viscous, and pale yellow in color. The pH of the solutions was in the range of 6.8–7.5. The in-situ gelling solutions containing 0.5% and above amount of calcium carbonate exhibited desired *in vitro* gelation property and also showed a long duration of floating on the surface of an acidic medium (pH 1.2). This could be due to the free availability of a sufficient number of calcium ions and carbon dioxide content from the calcium carbonate in an acidic medium to boost the gelling potential of sodium alginate and also induce floating

**Table 3.** Model summary statistics given by a Box–Behnken design.

Model	R <sup>2</sup>	Adjusted R <sup>2</sup>	Predicted R <sup>2</sup>	SD	% CV
Floating lag time					
Linear	0.9843	0.9801	0.9691	15.58	1.65
2FI	0.9864	0.9762	0.9388	17.00	
Quadratic	0.9997	0.9993	0.9957	3.01	
Viscosity					
Linear	0.5271	0.3981	0.0342	311.95	32.06
2FI	0.6399	0.3698	0.7200	319.20	
Quadratic	0.9102	0.7485	0.4373	201.66	
Cumulative % drug release (sixth hour)					
Linear	0.4576	0.3097	0.1265	7.10	6.95
2FI	0.6970	0.4697	0.4667	6.23	
Quadratic	0.9018	0.7251	0.5707	4.48	

\*Floating lag time = +170.00 – 144.75 A + 0.6250 B – 1.88 C + 3.75 AB + 1.75 AC + 8.50 BC + 24.50 A<sup>2</sup> – 1.25 B<sup>2</sup> 0.2500C<sup>2</sup>.

\*Viscosity = +440.00 – 124.87 A + 365.00 B + 17.38 C + 252.50 AB – 8.75 AC + 2.50 BC + 121.87 A<sup>2</sup> + 360.62 B<sup>2</sup> – 128.12 C<sup>2</sup>.

\*Drug release = +61.00 + 1.50 A – 7.50 B – 0.2500 C – 7.50 AB – 2.00 AC – 1.0000 BC + 1.50 A<sup>2</sup> – 2.00 B<sup>2</sup> + 7.00 C<sup>2</sup>.

characters in it. These findings are consistent with the reported results (Rajinikanth *et al.*, 2007).

The in-situ gels demonstrated a considerable increase in viscosity with increasing amount of sodium alginate. It was attributed to an increasing chain interaction with sodium alginate concentration. Similarly, an increase in the amount of calcium carbonate also increases the viscosity of the in-situ gels at all three sodium alginate percentage. It could be due to the high concentration of finely dispersed particles of calcium carbonate in the gelling solution. On the other hand, meloxicam has not contributed much in increasing the viscosity of in-situ gels as it was in its freely soluble ternary complex form with Hydroxypropyl-β-Cyclodextrin and diethanolamine.

A marked decline in the rate and extent of in-vitro drug release was noted with the increase in sodium alginate concentration in in-situ gels (Fig. 3). It is attributed to the high density of the system and also to the increase in the drug's diffusion path length. In order to study the drug release mechanism, the *in vitro* release data obtained were fitted to various kinetic equations. The release model of optimized in-situ gel formulation followed Matrix (Higuchi matrix) kinetics.

#### In-vivo anti-inflammatory activity

The optimized floating in-situ gel of MLX-HPβCD-DEA ternary complex has showed significant inhibition of carrageenan-induced rat paw edema from 2 to 6 hours in rats following oral administration, as compared with the control and standard group of animals. The highest percentage of inhibition of the standard drug pure meloxicam was found to be 59.37% ( $p < 0.05$ ), whereas the optimized floating in-situ gel of MLX-HPβCD-DEA ternary complex exhibited the maximum percentage of inhibition of paw edema at 6 hours is 84.38% ( $p < 0.05$ ) (Table 4), even though the standard drug has exhibited the significant inhibition of paw edema but the optimized gastric floating in-situ gel has been found to be more significant ( $p < 0.05$ ) paw edema inhibition from 2 hours to till 6 hours as compared to the control and standard group of animals.

#### Ulcerogenic study

The optimized gastric floating in-situ gel of meloxicam ternary complex and standard meloxicam showed significant ulcerogenic potential compared to control in rats treated with standard meloxicam/optimized formulation. The optimized formulation showed less ulcerogenic potential as compared to standard meloxicam (Fig. 4). These results clearly indicate that the optimized formulation could protect the gastric mucosa from injury (Fig. 5). Reduced gastric ulceration of the optimized formulation as compared with the standard could be due to the slow release of meloxicam from the in-situ gels (El-Kamel *et al.*, 2001).

#### CONCLUSION

The optimized gastric floating in-situ gel of Meloxicam-Hydroxypropyl-β-Cyclodextrin-Diethanolamine ternary complex demonstrated a desired gelling and floating property with the prolonged and acceptable amount of drug release in an acidic medium. Improved anti-inflammatory activity and reduced gastric ulceration of the optimized formulation as compared to the standard could be due to the use of a ternary complex of meloxicam in the formulation and prolonged release of meloxicam from the gastric floating in-situ gel, respectively. Thus, this gastric floating in-situ gelling system can be translated for existing and established NSAID as well as formulations.

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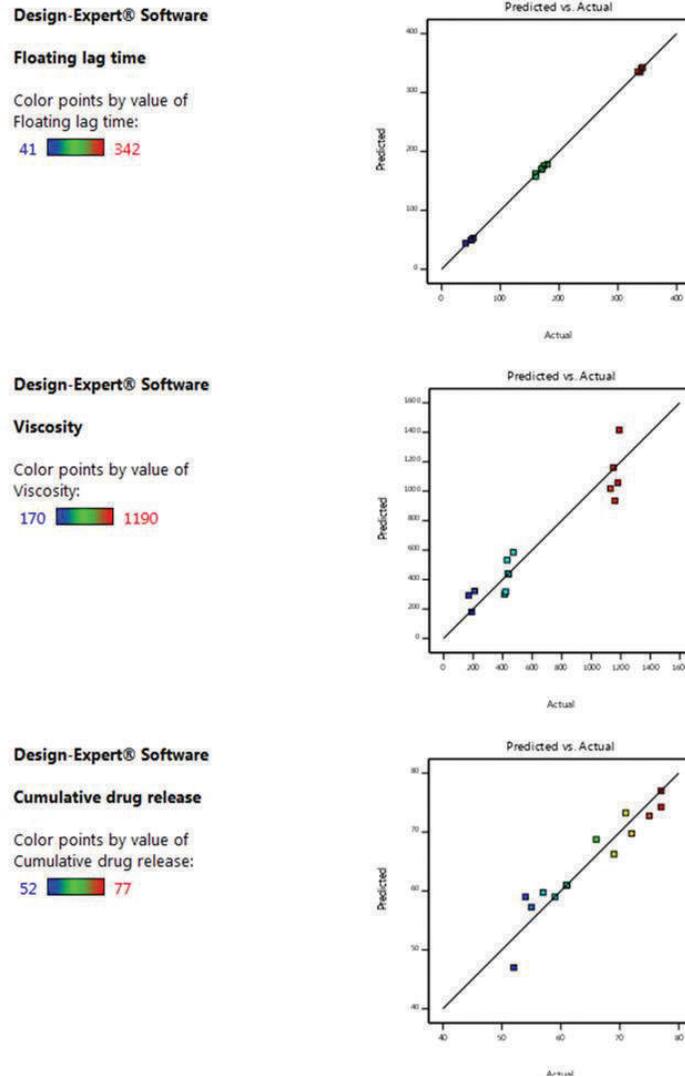


Figure 1. Actual vs Predicted values obtained from design expert software for gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

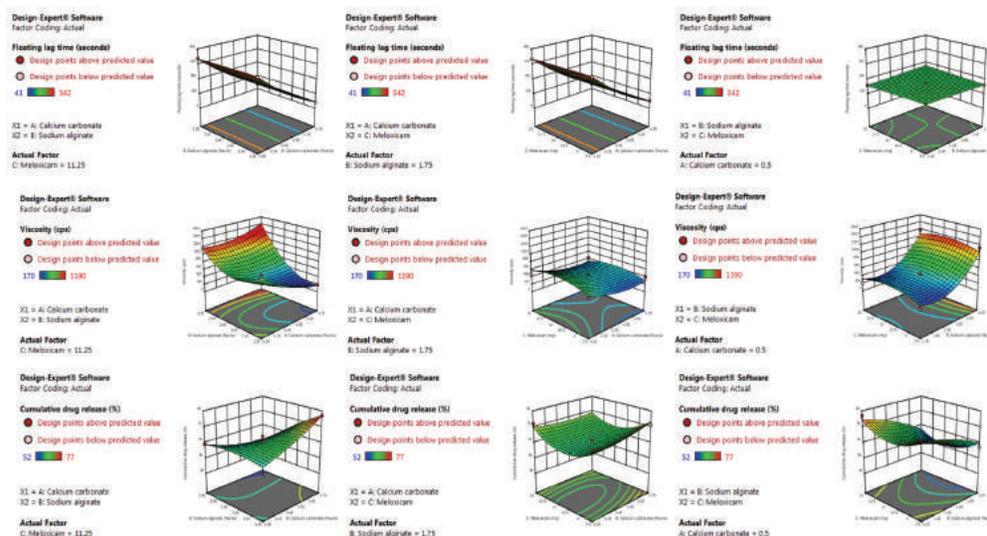


Figure 2. 3D graphs of independent variables floating lag time, viscosity, and cumulative drug release obtained from design expert software for gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

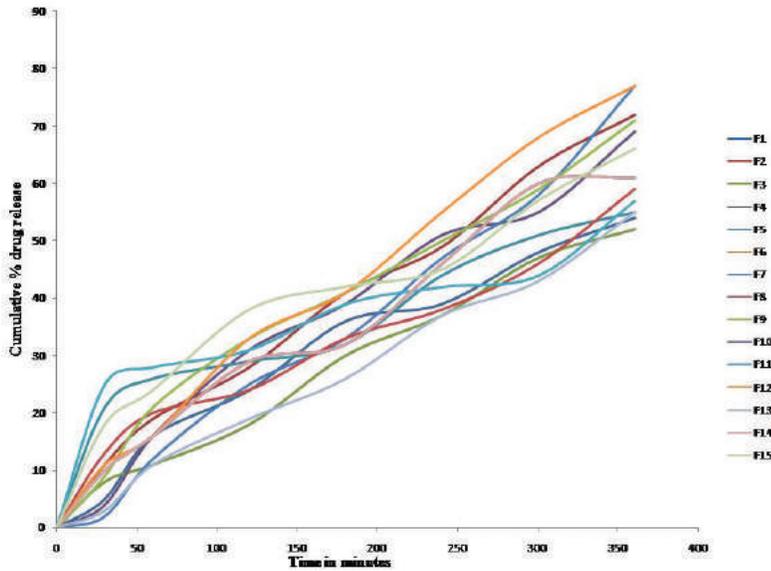


Figure 3. In-vitro drug release profile of gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

Table 4. Anti-inflammatory activity of optimized gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

Group	Treatment	Initial paw volume	Paw volume (ml)						Edema inhibition at sixth hour (%)
			1 hour	2 hours	3 hours	4 hours	5 hours	6 hours	
I	Control	1.17 ± 0.06	1.22 ± 0.02	1.47 ± 0.07	1.65 ± 0.07	1.67 ± 0.02	1.92 ± 0.04	2.18 ± 0.06	---
II	Standard	1.07 ± 0.09	1.18 ± 0.04	1.30 ± 0.03*	1.39 ± 0.05*	1.42 ± 0.01*	1.48 ± 0.05*	1.57 ± 0.01*	59.37
III	Optimized formulation	1.04 ± 0.02	1.17 ± 0.05	1.20 ± 0.01*	1.19 ± 0.02*	1.32 ± 0.06*	1.35 ± 0.03*	1.32 ± 0.04*	84.38

Values are presented as the mean ± SEM, n = 6 in each group; one-way ANOVA followed by multiple Tukey's comparison test. \*p < 0.05, as compared to the control group. ANOVA = analysis of variance; SEM = standard error of the mean.

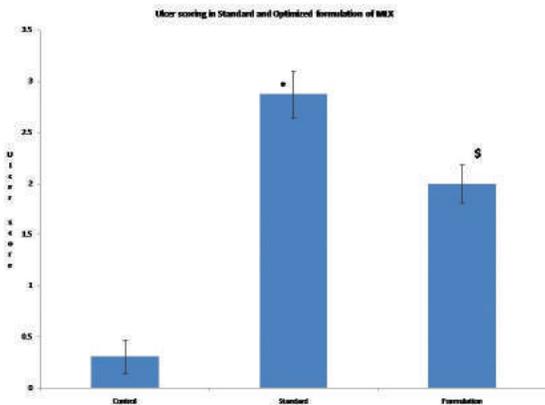


Figure 4. Ulcerogenic potential of pure meloxicam and optimized gastric floating in-situ gels of MLX-HPβCD-DEA ternary complex.

\*—Significant compared to control, \$—significant compared to standard drug group.

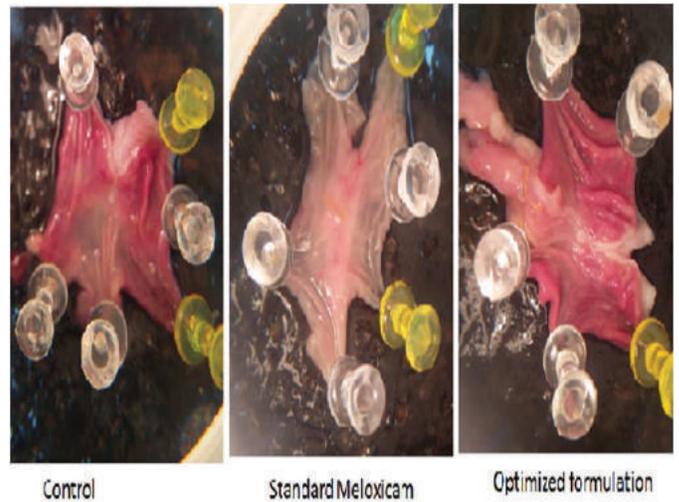


Figure 5. Representative stomachs of rats treated with pure meloxicam and optimized gastric floating *in-situ* gels of MLX-HPβCD-DEA ternary complex.

## DECLARATION OF INTEREST

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